Stochastic Modeling of Local and Global Intracellular Calcium Dynamics



Gregory D. Smith Department of Applied Science College of William and Mary







RyRs are clustered in cardiac myocytes (quarks, sparks, waves)

- Depolarization
- Ca influx (DHPRs)
- Ca release (RyRs)
- Elevated Ca in myoplasm
- Contraction of sarcomere

Sarcolemma Mvofilaments Contraction 200 ms

(Bers 2002)

"Common pool" models of excitation-contraction coupling do not properly account for local Ca signaling in the diadic space and junctional SR





$$\frac{\partial [\operatorname{Ca}^{2+}]}{\partial t} = D_{Ca} \nabla^2 [\operatorname{Ca}^{2+}] - k_f [\operatorname{Ca}^{2+}] [\mathrm{B}] + k_r [\operatorname{Ca}^{\mathrm{B}}] + \sigma(t) \delta(r)$$
$$\frac{\partial [\mathrm{B}]}{\partial t} = D_B \nabla^2 [\mathrm{B}] - k_f [\operatorname{Ca}^{2+}] [\mathrm{B}] + k_r [\operatorname{Ca}^{\mathrm{B}}]$$
$$\frac{\partial [\operatorname{Ca}^{\mathrm{B}}]}{\partial t} = D_{CaB} \nabla^2 [\operatorname{Ca}^{\mathrm{B}}] + k_f [\operatorname{Ca}^{2+}] [\mathrm{B}] - k_r [\operatorname{Ca}^{\mathrm{B}}]$$

r = 0: flux for Ca turns "on" at t = 0 (no flux for buffer) $r \rightarrow \infty$: buffers in equilibrium with background Ca 5 pA source — cluster of channels — fast buffer kinetics



0.5 pA source — single channel — slow buffer kinetics



• Steady-state rapid buffer limit (large source)

$$D_{Ca}[Ca^{2+}] + D_{CaB} \frac{[Ca^{2+}][B]_{T}}{[Ca^{2+}] + K} = \frac{\sigma}{2\pi r} + const$$
$$K = k_r/k_f \qquad [B]_{T} = [B] + [CaB]$$

Buffer is nearly saturated near source Local equilibrium between Ca^{2+} and buffer everywhere

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(Wagner & Keizer 1994)
     (Smith 1996)
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Steady-state excess buffer limit (small source)

$$[\operatorname{Ca}^{2+}] = \frac{\sigma}{2\pi D_{Ca} r} e^{-r/\lambda} + [\operatorname{Ca}^{2+}]_{\infty}$$
$$\lambda = \sqrt{D_{Ca}/k_f[B]_{\infty}} \quad [B]_{\infty} = \frac{K[B]_T}{[\operatorname{Ca}^{2+}]_{\infty} + K}$$



Buffer profile is only slightly perturbed near source No local equilibrium between Ca^{2+} and buffer near source

(Neher 1986)



Time: 0.00 msec

10³



[CaB] [Ca] [Ca]bc

 $\rightarrow \infty$

·--[B]

IP3R and RyR gating modeled as a Markov chain



Control



intracellular channels are modeled as Markov chains

$$X(t) \in \{1, 2, \cdots, M - 1, M\}$$

each state is "open" or "closed"



improve next slide

four-state model with fast Ca activation and slow Ca inactivation





four-state model with fast Ca activation and slow Ca inactivation



two-state model with Ca activation but no inactivation



channels are coupled assuming excess buffer limit

$$C = (c_{ij})$$

N×N coupling matrix

$$c_{ij} = \frac{\sigma_O}{2\pi D r_{ij}} e^{-r_{ij}/\lambda}$$

superpose interactions

instantaneous coupling $au_{chan} << au_{diff}$

arrangement of channels

 $\mathbf{R} = \mathbf{0.12} \lambda$ Score = 0.47 Time = 0 msN_c No N_R CCC $O_1 \xrightarrow{B} C$ C C C C C C C C C C n Ca 🖌 n Ca Popen СССС D C₃ \mathbf{C}_{1} CCC Ca m Ca

Four-state model with Ca²⁺ activation and Ca²⁺ inactivation

Four-state model with Ca²⁺ activation and Ca²⁺ inactivation



accumulation of Ca inactivation leads to termination of these puffs



Limiting probability distributions



Not all parameters lead to puffs (*Score* > 0.3) but parameters leading to puffs are easy to find





Two-state model with Ca^{2+} activation but no Ca^{2+} inactivation



Puffs are sensitive to channel density (w/o Ca inactivation)



Puffs terminating via Ca inactivation are not sensitive to channel density



Parameter studies are performed using direct methods

$$\pi^T Q^{(N)} = 0$$
 subject to $\pi^T e = 1$

— nontrivial due to state space explosion —



"mean-field" approximation for channel coupling

Coupling matrix $C = (c_{ij})$ gives [Ca] increase experienced by channel j when channel i is open



Mean-field approximation usually works well (see next slide)

Open symbols are full model while X's are mean-field result



The details of channel position are important primarily through their effect on the average coupling stength (c*)

Isn't stochastic attrition an unlikely termination mechanism?



The time constant for stochastic attrition is an exponential function of the number of open channels

$$\tau_{attrit} = \frac{1}{k_{attrit}} = \tau_O \frac{1 - (1 - p_O)^N}{N(1 - p_O)^{N-1} p_O} \qquad p_O = \frac{\tau_O}{\tau_C + \tau_O}$$

(Stern)



The time constant for stochastic attrition depends on the coupling strength (i.e., the density of the release site)

$$\tau_{attrit} = \frac{1}{k_{attrit}} = \frac{1}{k_{-}} \left\{ 1 + \sum_{i=1}^{N-1} \left[\frac{(N-1)!}{(i+1)!(N-1-i)!} \prod_{j=1}^{i} \left(\frac{c_{\infty} + jc_{*}}{K} \right)^{\eta} \right] \right\}$$



But stochastic attrition is not robust when the number of channels is large, that is, it requires channels with precisely the right density or source amplitude

One expects that the time constant for domain formation and collapse will influence puff/spark termination

Before considering Ca release sites, consider the effect of a time-dependent Ca domain on a single Ca-regulated channel

Effect of "residual calcium" on Ca-regulated channels



$$\frac{dc}{dt} = \alpha(t) - \frac{c - c_{\infty}}{\tau} \quad \text{where} \quad \alpha(t) = \begin{cases} 0 & \text{when} & S(t) = C\\ \alpha_0 & \text{when} & S(t) = O. \end{cases}$$
$$c_{\infty} < c < c_{ss} = \tau \alpha_0 + c_{\infty}$$

Effect of "residual Ca" on Ca-activated channel



when domain is slow "residual calcium" from previous openings increases rate of $C \rightarrow O$ transitions leading to elevated open probability Probability density approaches as an alternative to Monte Carlo

The joint distributions

$$\rho_C(c,t)dc = \mathsf{P}\left\{c < [\mathsf{Ca}^{2+}] < c + dc \text{ and } S(t) = C\right\}$$

$$\rho_O(c,t)dc = \mathsf{P}\left\{c < [\mathsf{Ca}^{2+}] < c + dc \text{ and } S(t) = O\right\}$$

are time-dependent and satisfy

reaction (stochastic gating)



advection (deterministic dynamics of domain)

$$\phi_C(c,t) = j_C(c)\rho_C(c,t) \qquad j_C(c) = -\frac{c-c_\infty}{\tau}$$

$$\phi_O(c,t) = j_O(c)\rho_O(c,t) \qquad j_O(c) = \alpha_0 - \frac{c-c_\infty}{\tau}$$

Time-dependent probability densities



The PD approach w/ more complicated single channel models



$$\rho_{i}(c,t)dc = \mathsf{P}\left\{c < [\operatorname{Ca}^{2+}] < c + dc \\ \text{and } S(t) = \mathcal{S}_{i}\right\}$$
$$\frac{\partial \rho}{\partial t} = -\frac{\partial}{\partial c}\left[\rho J\right] + \rho Q$$
$$\rho = (\rho_{1}, \rho_{2}, \cdots, \rho_{M})$$

$$\begin{array}{c|c} \tau \text{ small} \\ \rho_{C_1} & 0.72 \\ \hline \rho_{O} & 0.09 \\ \hline \rho_{C_2} & 0.02 \\ \hline \rho_{C_3} & 0.17 \end{array}$$

The PD approach to study the effect of "lumenal depletion"



$$\frac{dC_{cyt}}{dt} = \gamma(t)\nu_{rel}(C_{er} - C_{cyt}) - \nu_{dom}(C_{cyt} - C_{min})$$
$$\frac{dC_{er}}{dt} = \frac{1}{\lambda} \left[-\gamma(t)\nu_{rel}(C_{er} - C_{cyt}) + \nu_{dom}^{er}(C_{max} - C_{er})\right]$$

The joint probability densities become multivariate

$$\rho_i(C_{cyt}, C_{er}, t) \ dC_{cyt} \ dC_{er} = \operatorname{Prob}\{C_{cyt} < \tilde{C}_{cyt} < C_{cyt} + dC_{cyt} \ \operatorname{AND} C_{er} < \tilde{C}_{er} < C_{er} + dC_{er} \ \operatorname{AND} \gamma(t) = i\}$$

but still satisfy a system of advection-reaction equations

$$\frac{\partial}{\partial t}\rho_i = \frac{\partial (F_{cyt}^i \rho_i)}{\partial C_{cyt}} - \frac{\partial (F_{er}^i \rho_i)}{\partial C_{er}} + [\vec{\rho}\mathbf{Q}]_i$$

The probability flux has two components

$$F_{cyt}^{i} = \gamma_{i} \nu_{rel} (C_{er} - C_{cyt}) - \nu_{dom} (C_{cyt} - C_{min})$$

$$F_{er}^{i} = \frac{1}{\lambda} \left[-\gamma_{i} \nu_{rel} (C_{er} - C_{cyt}) + \nu_{dom}^{er} (C_{max} - C_{er}) \right]$$

each of which depends on channel state

Cytosolic domain and lumenal depletion domain Ca-activated channel

fast domain (large v's)

slow channel



fast channel







Ca_{cyt}

Comparison of Monte Carlo and probability density approaches



Calcium activated channel — effect of lumenal depletion



Dynamics of spark termination — effect of lumenal depletion



A new class of whole cell models

 ∂

 $\partial \boldsymbol{\rho}$



$$\frac{1}{\partial t} = -\overline{\partial c} \left[\rho J \right] + \rho Q$$

$$\frac{dc_{cyt}}{dt} = J_{cyt}^* + J_{leak} - J_{pump}$$

$$\frac{dc_{er}}{dt} = \frac{1}{\lambda_{er}} \left(J_{pump} - J_{leak} - J_{er}^* \right)$$

$$J_{cyt}^* = \sum_{i=1}^{M} \int_{c_{2}^{min}}^{c_{2}^{max}} \int_{c_{1}^{min}}^{c_{1}^{max}} v_{cyt}(c_{1} - c_{cyt})\rho_{i}(c_{1}, c_{2})dc_{1}dc_{2}$$

$$J_{er}^* = \sum_{i=1}^{M} \int_{c_{min}}^{c_{2}^{max}} \int_{c_{min}}^{c_{1}^{max}} v_{er}(c_{er} - c_{2})\rho_{i}(c_{1}, c_{2})dc_{1}dc_{2}$$

large number of channels each with it's own time-dependent domain

Diffuse IP3Rs with time-dependent domains



New approach for modeling "local control" during EC coupling



SFU model (both closed) CC k_{ryr}^+ = CO (RyR open) $k_{ryr}^ k_{dhpr}^ 1 \downarrow k_{dhpr}^+$ (DHRP open) OC k_{ryr}^+ OO (both open) k_{ryr}^+ $k_{ryr}^ k_{ryr}^ k_{ryr}^-$



Monte Carlo simulation of voltage-clamped cardiac myocyte



Marginal densities show lumenal depletion during voltage step



JSR is slow compared to diadic subspace...

Because JSR is slow compared to diadic subspace, we can reduce to one-dimensional densities (in terms of Cajsr)



Probability density approach exhibits "gain and gradedness"



Computational efficiency of Monte Carlo and probability density approaches

Assuming the large N limit is of interest (20,000 SFUs ≈ infinity)

Monte Carlo approach

discretization error time step (∆t) number of SFUs (N) Probability density approach

discretization error time step (Δt) resolution of mesh (Δc)





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